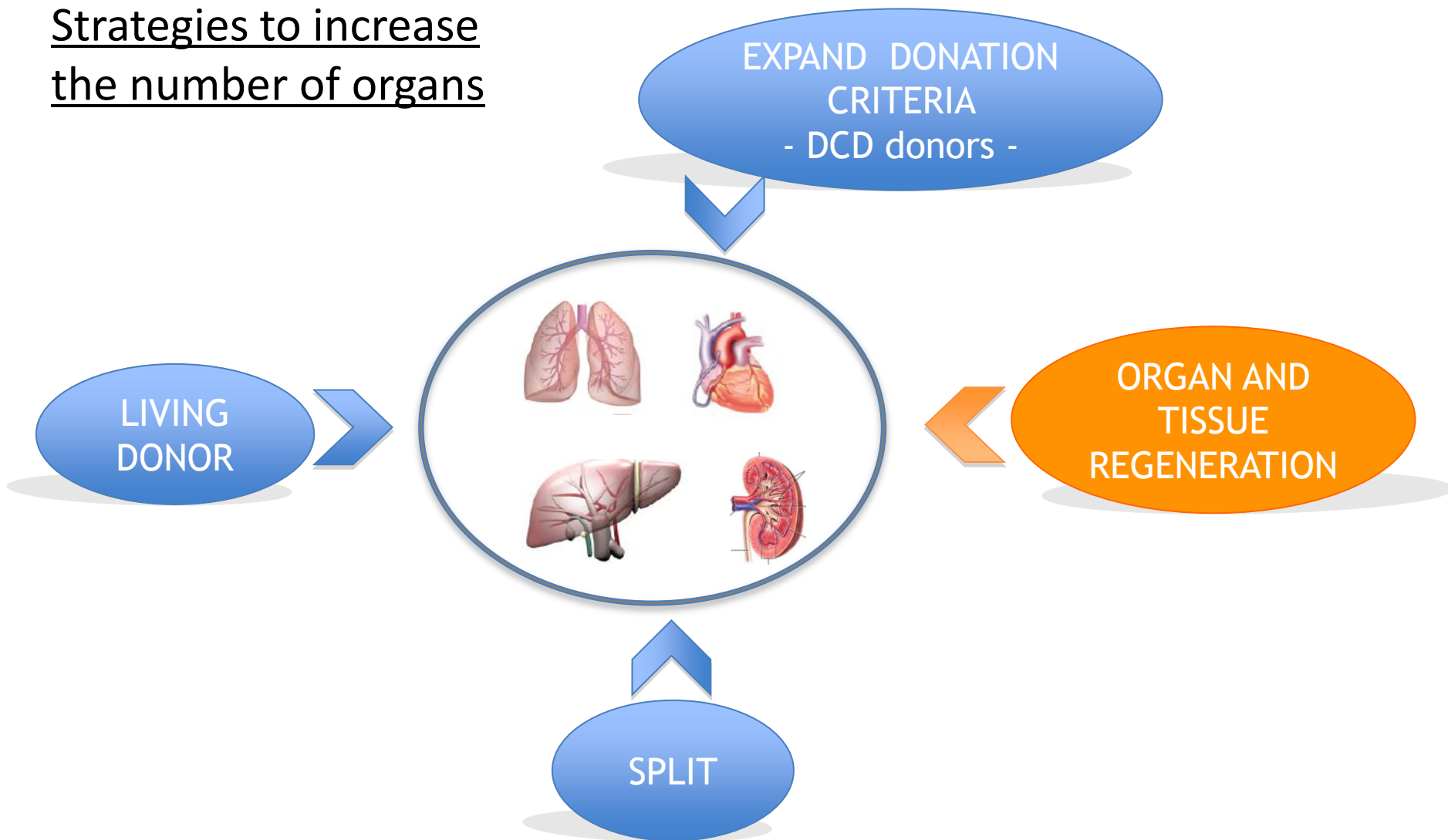




Present and future of regenerative medicine

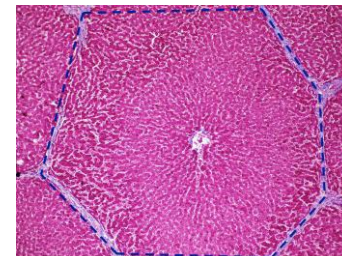
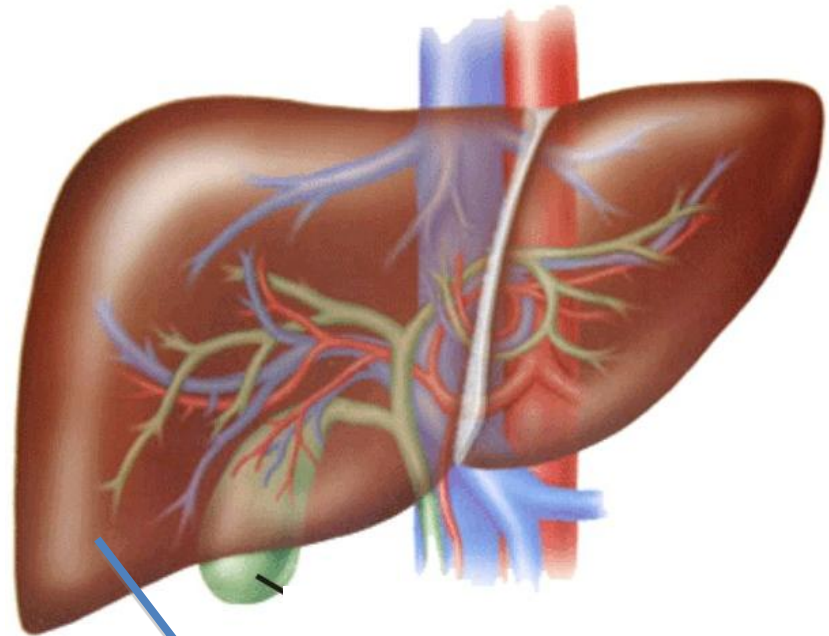
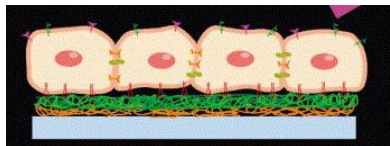
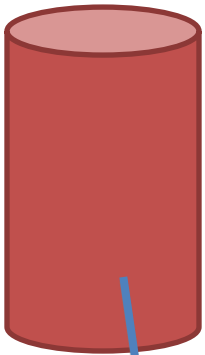
Liver Transplantation

Strategies to increase the number of organs



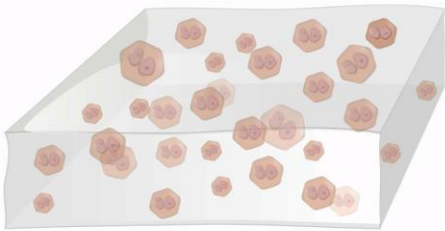
Solid organs: structural complexity!!

Traquea
Urine Bladder



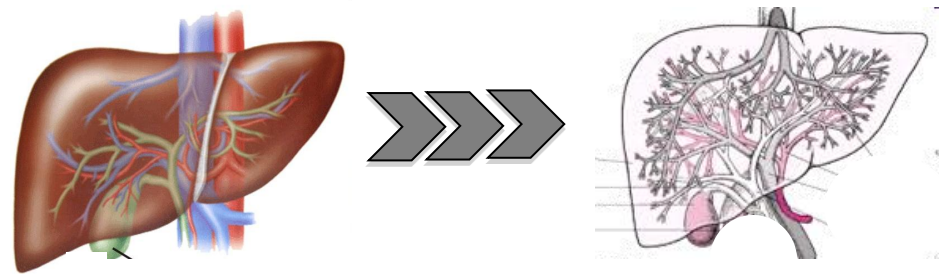
Ideal scaffold : biocompatibility, biodegradability, porosity, structural support

Artificial Scaffold



- Difficult control of size, microarchitecture and interconnectivity of pores

Natural Scaffold



Organ

Extracellular Matrix

- Physical, chemical and molecular stimuli that enable cell engraftment
- Preservation of vascular network
- Low immunogenicity

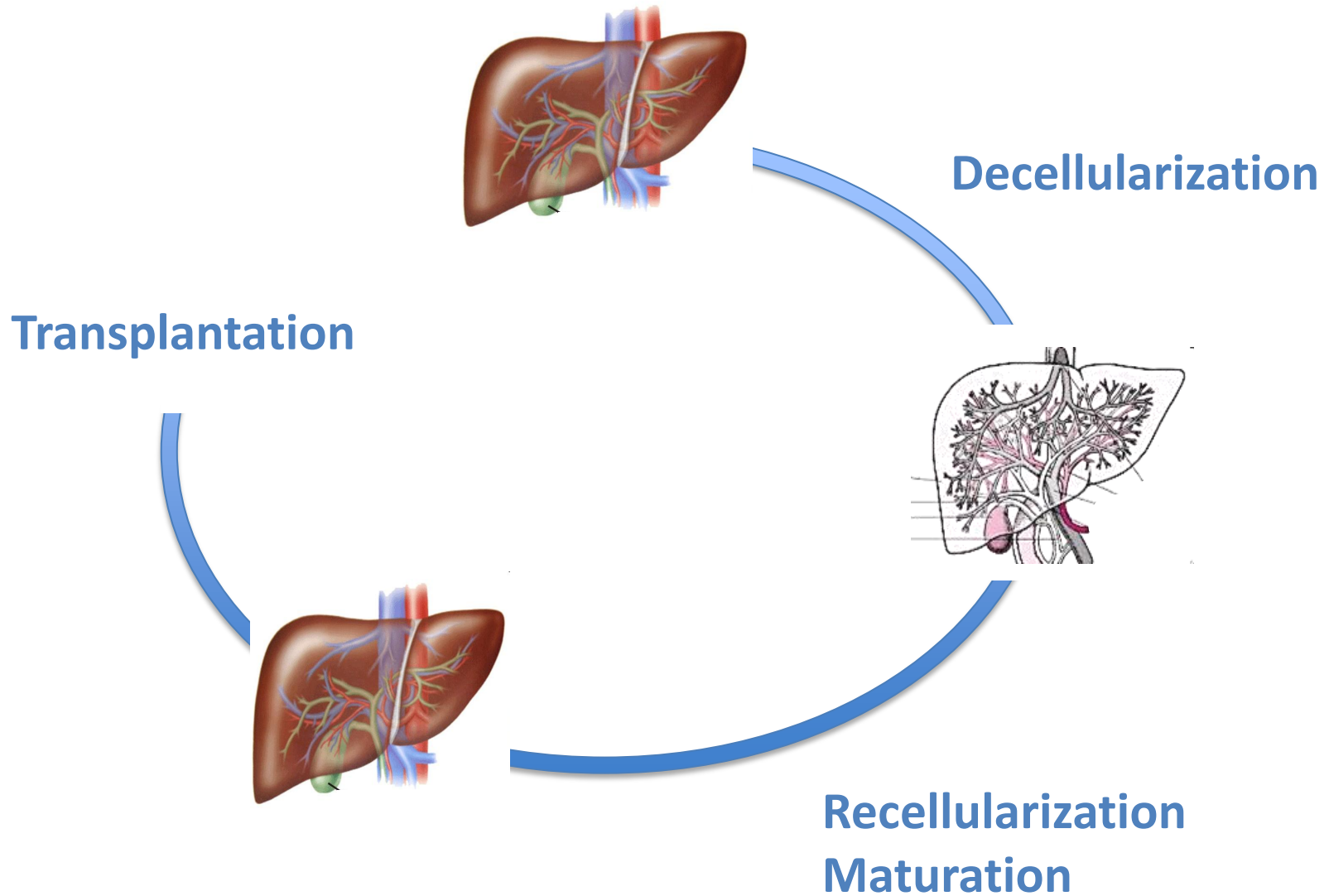


Table 1. Studies in the literature

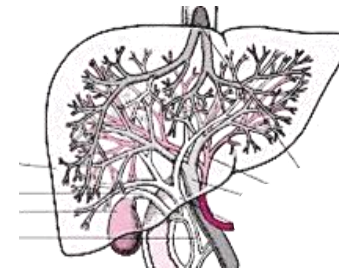
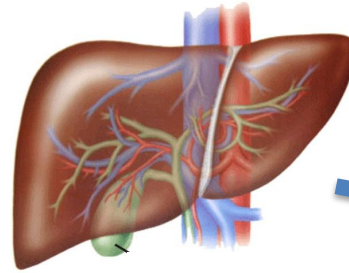
Author	Type Cells	Infusion Method	Via	Number Cells	Flow Rate	Time
Baptista 2010	hUVEC hFLC MS1	Continuous	PV IVC, PV, IVC+PV	30x10 ⁶ 70 x10 ⁶ 100 x10 ⁶	3ml/min → 0.5ml/ min 5ml/min	7d 3d
Uygun 2010	Rat MH Endothelial cells	Multistep	PV	200 x10 ⁶	15ml/min	5d 5d
Soto 2011	Rat MH	Direct injection Continuous Multistep	PV	10–50 x10 ⁶	2ml/min	7d
Yagi 2013	Pig MH	Multistep	PV	100 x10 ⁶	4ml/min	7d

Table 2. Culture media used by different authors

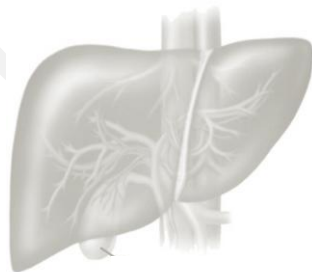
Author	Media
Baptista 2010 ¹	RPMI 1640, FBS, dexamethasone, penicillin-streptomycin, prolactin, glucagon, niacinamide, lipoic acid, triiodothyronine, hEGF, hHDL, hHGF, hGH, insulin, transferrin
Uygun 2010 ³	William's E, FBS, insulin, EGF, glucagon, hydrocortisone, penicillin-streptomycin
Soto 2011 ⁶³	EMEM, EGF, HGF, dexamethasone, insulin, human transferrin, selenous acid supplement, penicillin-streptomycin
Yagi 2013 ⁶³	DMEM, EGF, hidrocorcortisone, insulin, glucagon, penicillin-streptomycin

Caralt M. Organogenesis 2014;10(2):250

Decellularization



Transplantation



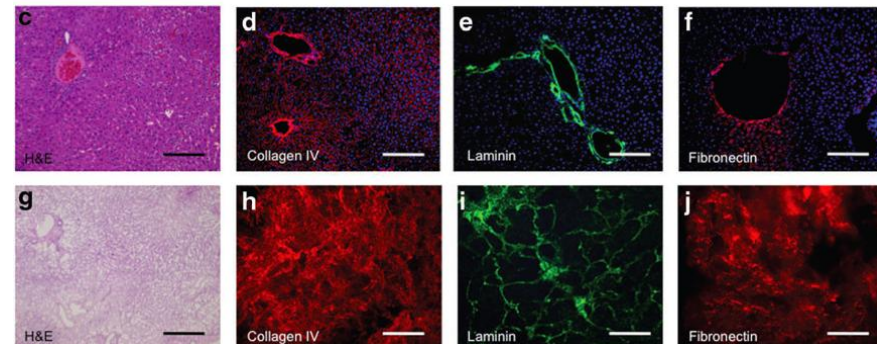
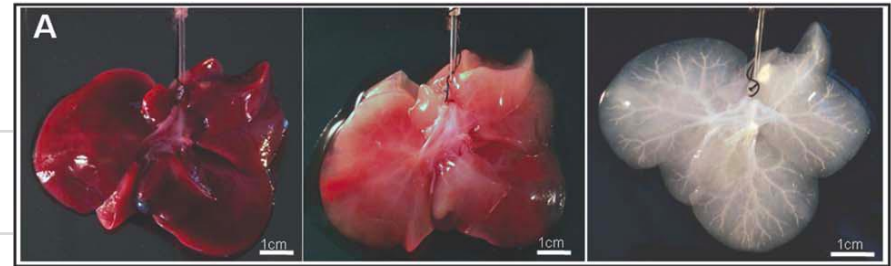
Recellularization
Maturation

Different decellularization “recipes” in liver

Uygun	rat	SDS Triton X-100	0.01% 24h, 0.1% 24h, 1% 24h 1% 30min	1ml/min
Baptista	rat	Triton X-100 + NH4 OH	1%+3%, 3h	5ml/min
Soto	rat	Trypsin + EGTA Triton X-100 + EGTA	0.02%+0.05%, 2h 3%+0.05%, 24h	8ml/min
Bao	rat	Adenosine SDS	10mM 1% 4h, 0.5% 4h, 0.25% 4h	25ml/min
Yagi	pig	SDS Triton X-100	0.01% 24h, 0.1% 24h, 1% 48h 1% 30min	30ml/min
Ko	pig	Triton X-100 + NH4 OH	1%+3%, 3h	0.5ml/min

Different decellularization “recipes” in liver

Uygun	rat	SDS Triton X-100
Baptista	rat	Triton X-100 + NH ₄ OH
Soto	rat	Trypsin + EGTA Triton X-100 + EGTA
Bao	rat	Adenosine SDS
Yagi	pig	SDS Triton X-100
Ko	pig	Triton X-100 + NH ₄ OH



... best decellularization protocol in kidneys

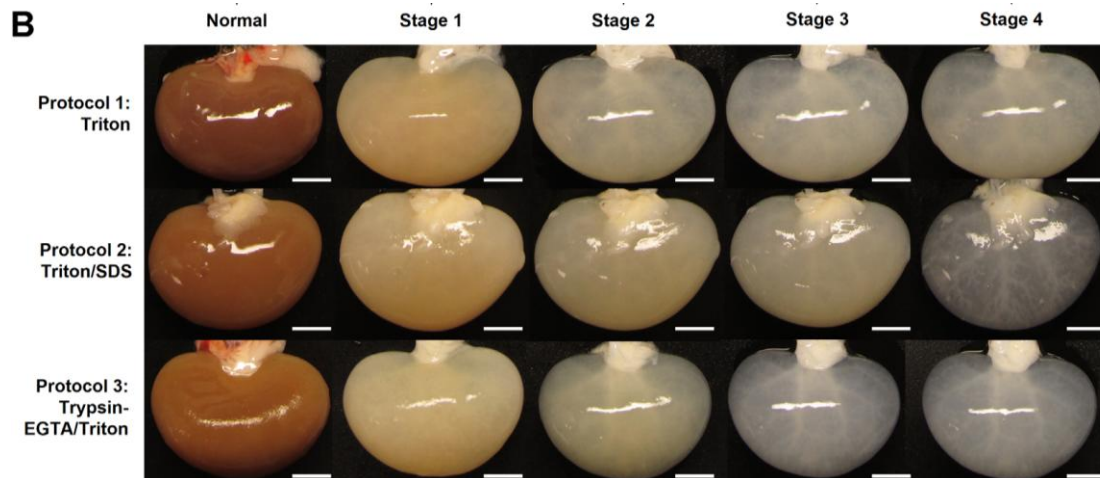
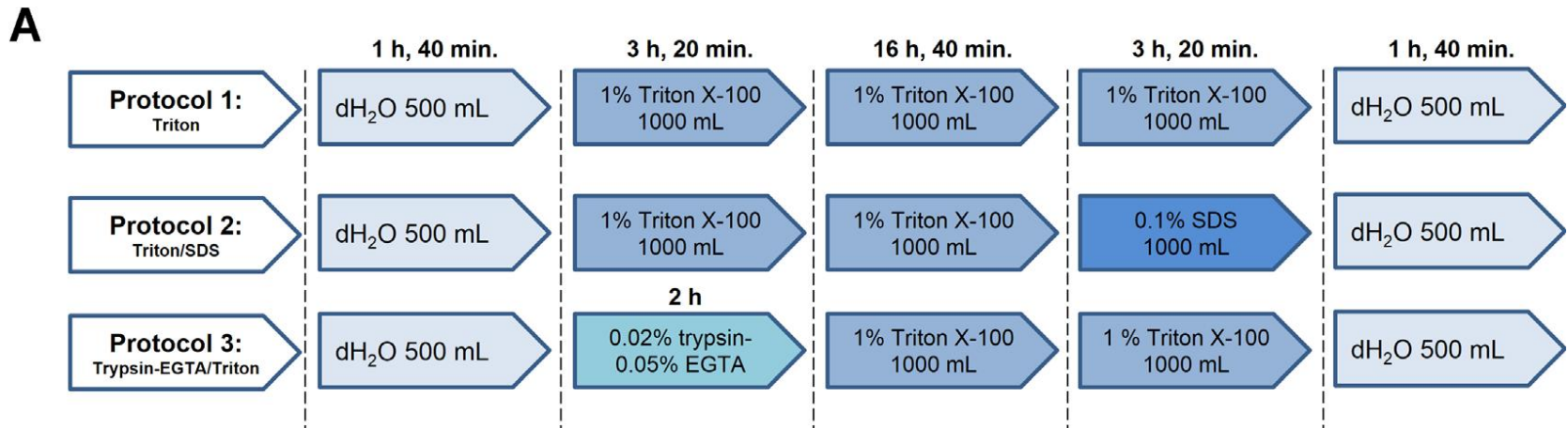
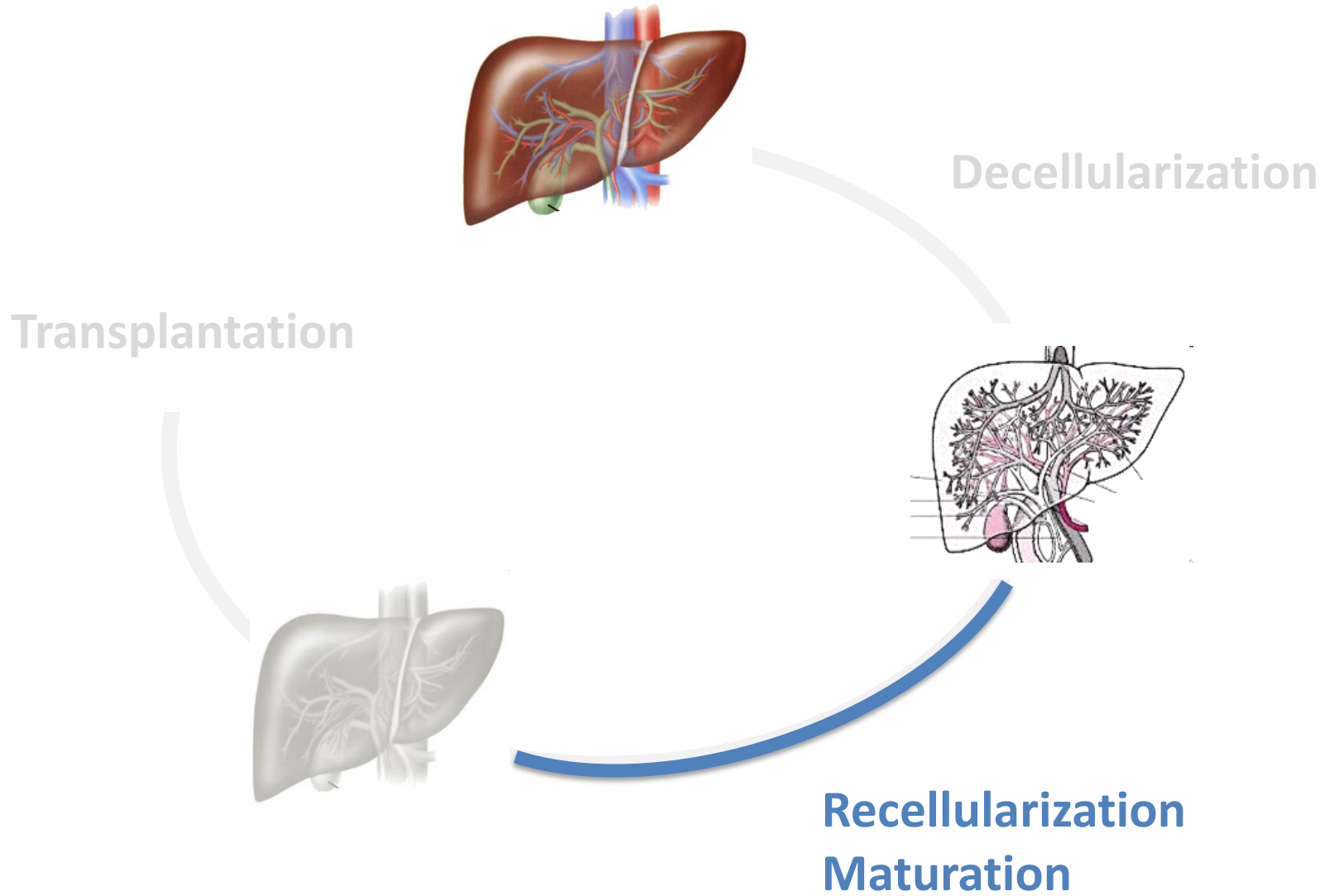


Table 1: Summary evaluation of decellularization protocols

Selection criteria	Protocol 1: Triton	Protocol 2: Triton/SDS	Protocol 3: Trypsin-EGTA/Triton
Macroscopic appearance (transparency of gross tissue is the goal)	-	+	+
Microscopic appearance (H&E, SEM, cell removal, maintenance of architecture is goal)	-	+	+/-
DNA reduction (goal: >95%)	-	+	-
Nuclear basophilia score (goal score is 1.0-2.0)	- Glomeruli: 2.1 ± 0.4; Tubules: 1.9 ± 0.9; Vessels: 3.4 ± 0.8	+ Glomeruli: 1.0 ± 0.0; Tubules: 1.0 ± 0.0; Vessels: 1.0 ± 0.0	+ Glomeruli: 1.1 ± 0.4; Tubules: 1.1 ± 0.4; Vessels: 1.3 ± 0.8
Architectural score (goal score is 4.0-5.0)	+ Glomeruli: 4.3 ± 0.5; Tubules: 4.4 ± 0.8; Vessels: 5.0 ± 0.0	+ Glomeruli: 4.0 ± 0.6; Tubules: 4.2 ± 0.8; Vessels: 5.0 ± 0.0	+ Glomeruli: 3.9 ± 0.7; Tubules: 4.1 ± 0.4; Vessels: 5.0 ± 0.0
ECM (collagen, laminin) retention (goal is retention of proteins)	+	+/-	+/-
Growth factor (bFGF, VEGF) retention (goal: >30% retention)	+	+	-

bFGF, basic fibroblast growth factor; ECM, extracellular matrix; H&E, hematoxylin & eosin; SEM, scanning electron microscopy; SDS, sodium dodecyl sulfate; VEGF, vascular endothelial growth factor.

For each criterion, protocols were evaluated and assigned one of three values: good (+), fair (+/-) or poor (-) at reaching a target goal. Each protocol was evaluated independently of the other two protocols, and is compared to normal kidneys.



Organ reengineering through development of a transplantable recellularized liver graft using decellularized liver matrix

Basak E Uygun¹

NATURE MEDICINE VOLUME 16
NUMBER 7 | JULY 2010

Primary rat hepatocytes

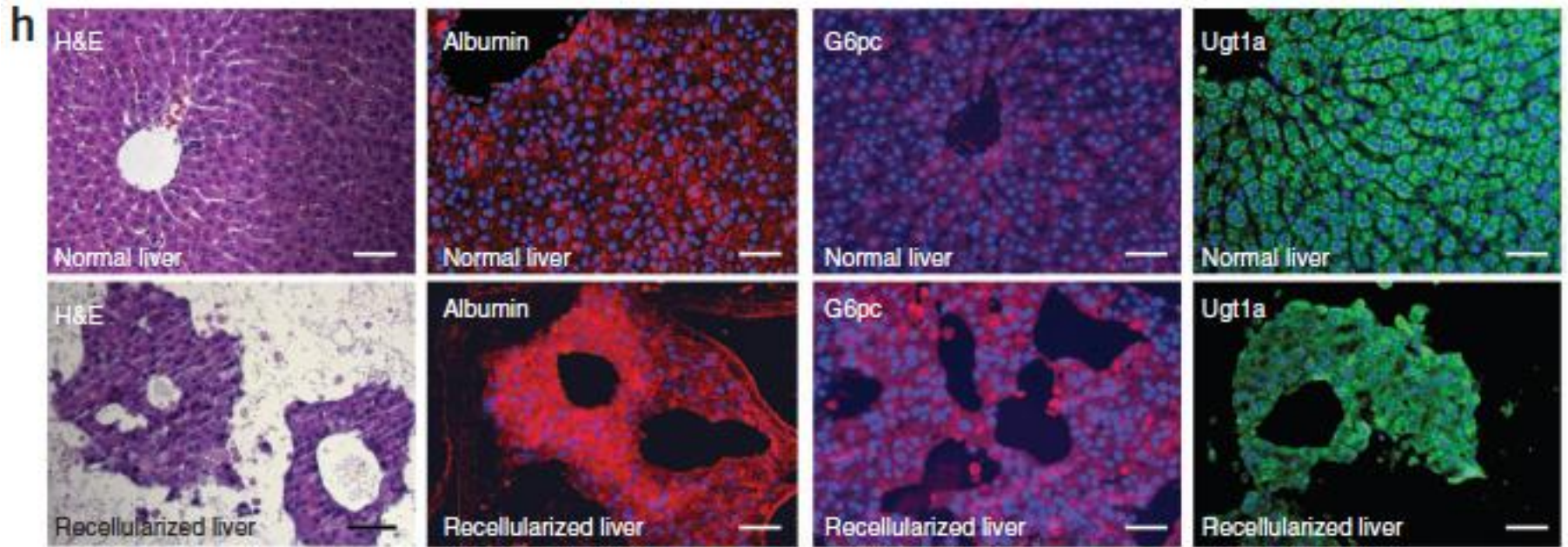


The Use of Whole Organ Decellularization for the Generation of a Vascularized Liver Organoid

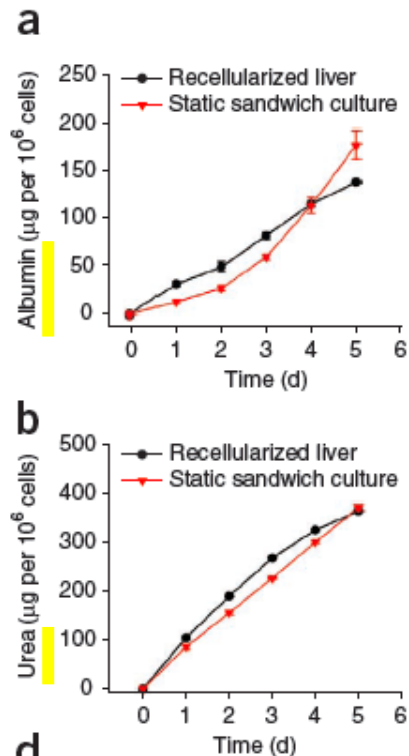
BAPTISTA ET AL. HEPATOLOGY, Vol. 53, No. 2, 2011

hFLCs + hUVEC

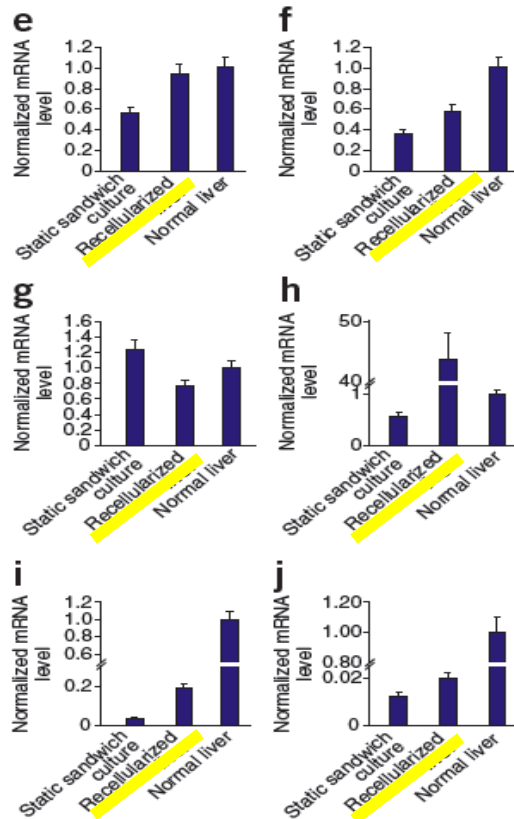




Uygun. Nature 2010;16(7):814-821

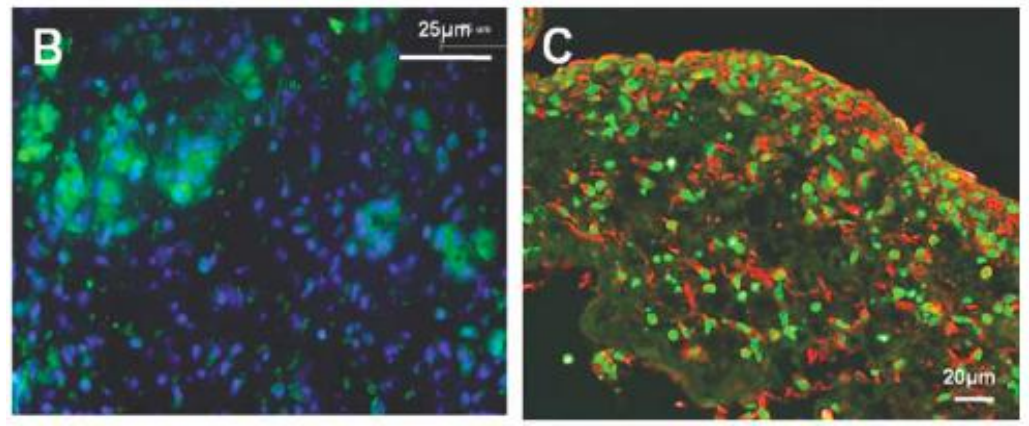
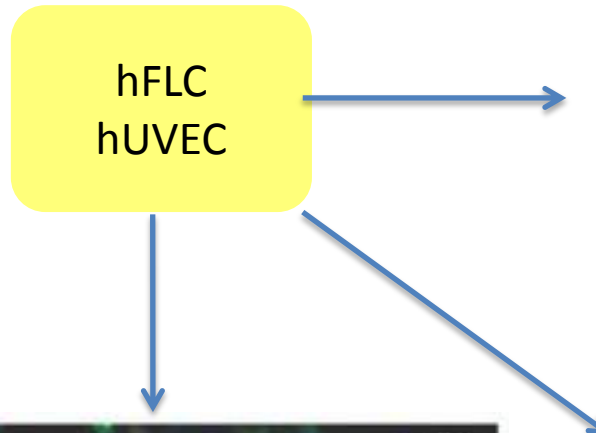


20% albumin production of *in vivo* levels

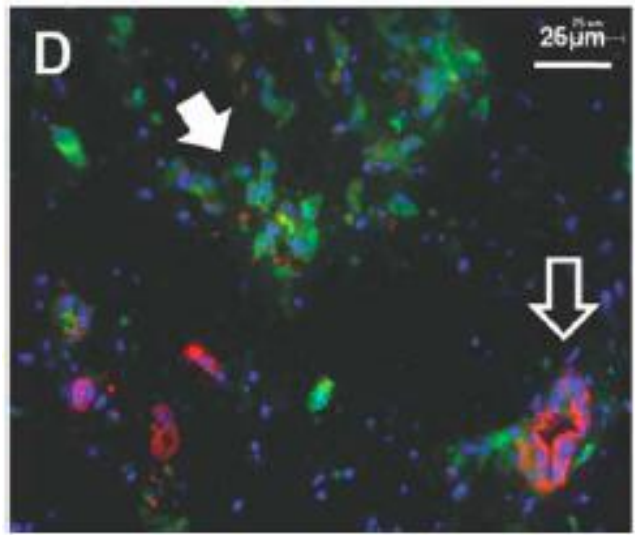


(e-j) Normalized gene expression of *Cyp2c11* (e), *Gstm2* (f), *Ugt1a1* (g), *Cyp1a1* (h), *Adh1* (i) and *Cyp3a18* (j). All error bars represent s.e.m. (n = 3).

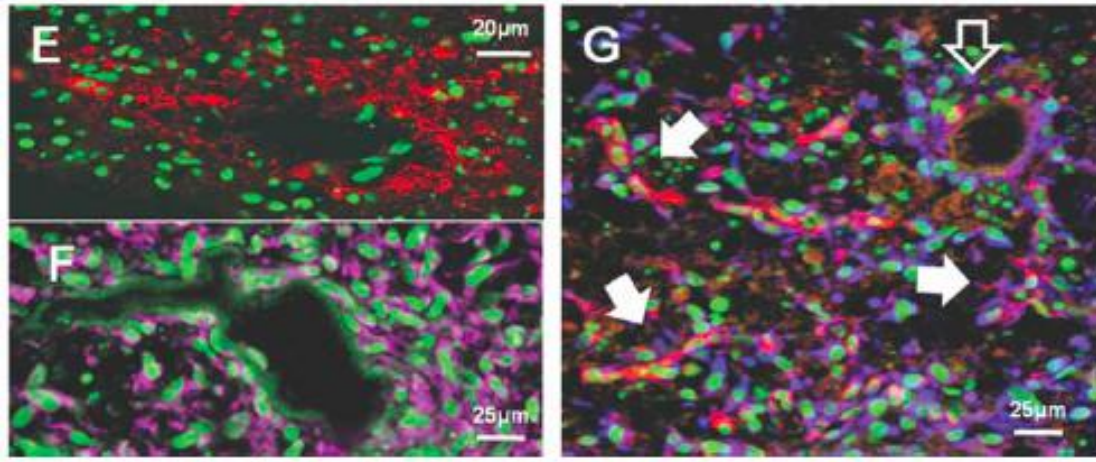
30% drug metabolism gene expression of *in vivo* levels



p450 CYP2A (green) and p450 CYP3A (red)

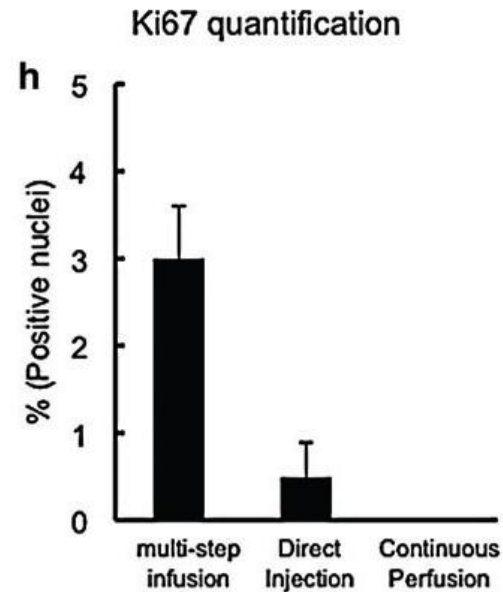
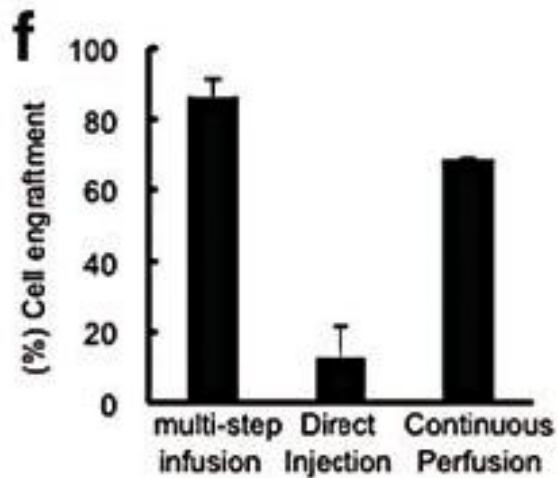


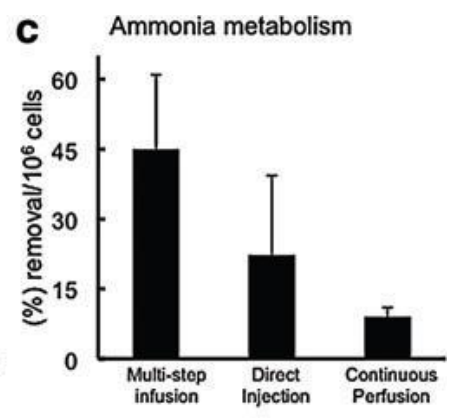
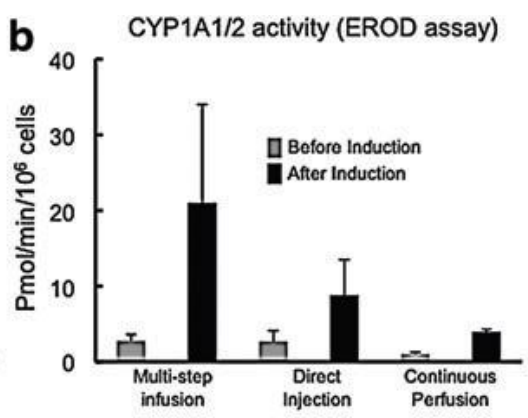
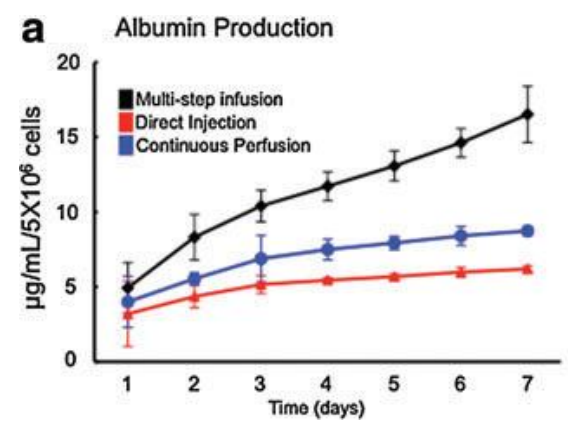
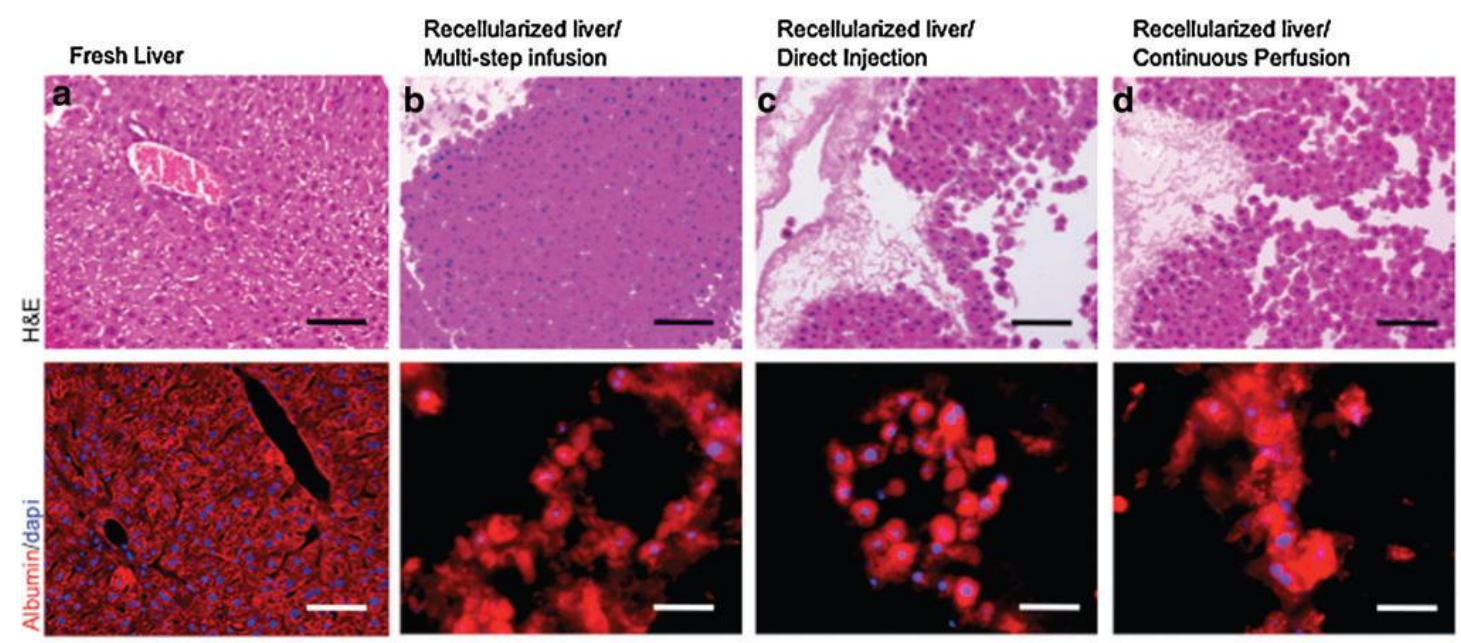
CK 19 (red) and albumin (green)

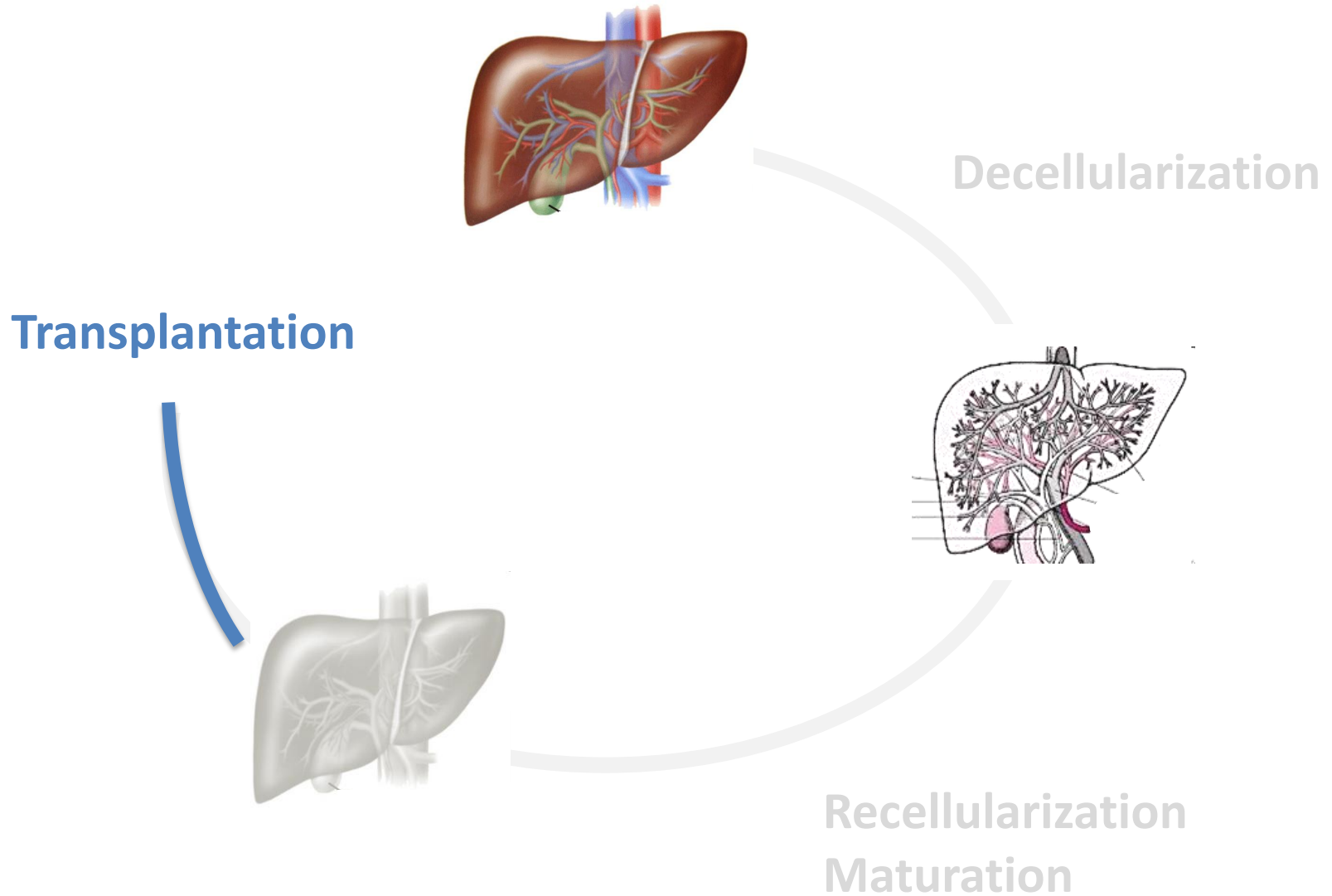


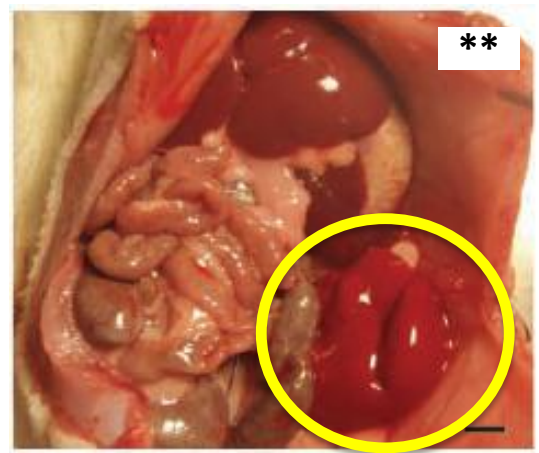
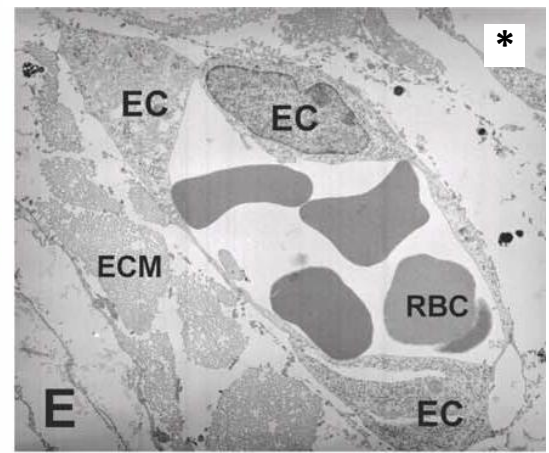
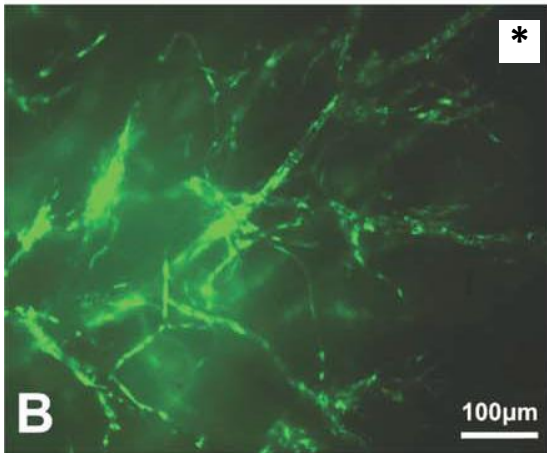
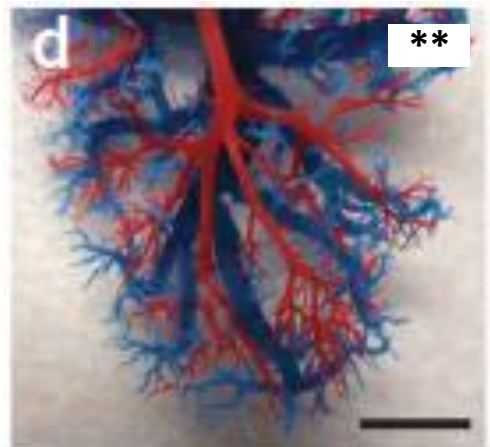
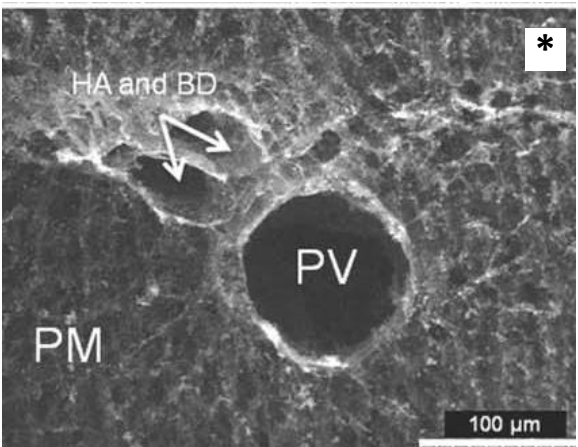
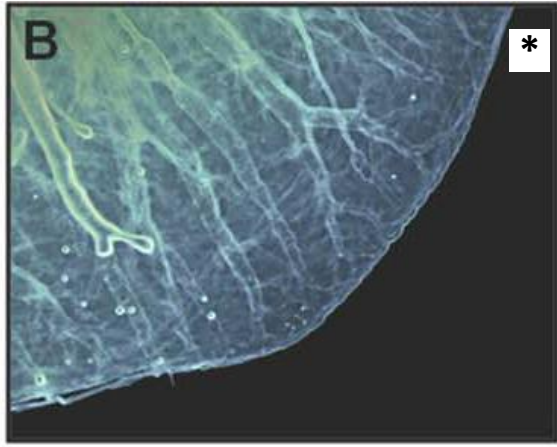
Von Willebrand (red) and endothelial oxid nitric synthetase (pink)

Direct parenchymal injection	Continuous perfusion	Multistep infusion
Direct injections into different lobes	Cells suspended in culture media	Cells through Porta Vein 4 steps at 10-15min interval





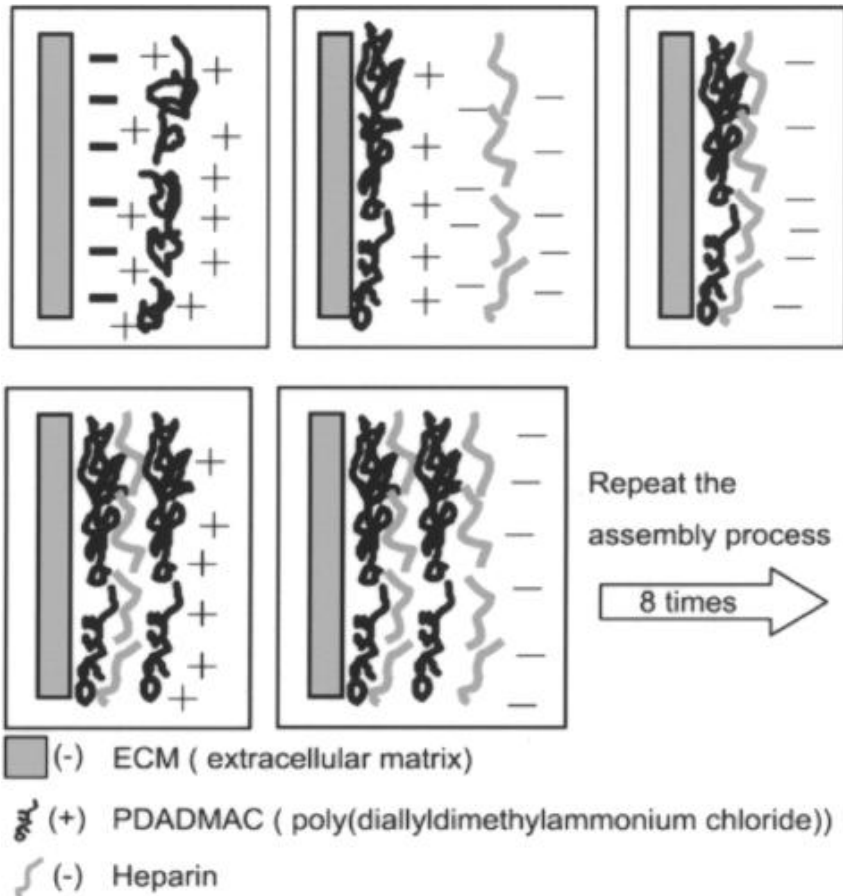




8h viability
thrombosis

* Baptista et al. Hepatology 2010;12:604-617

** Uygun. Nature 2010;16(7):814-821



LbL self-assembly technique

Polyelectrolyte
polydiallyldimethylammonium chloride
(PDADMAC) positively charged

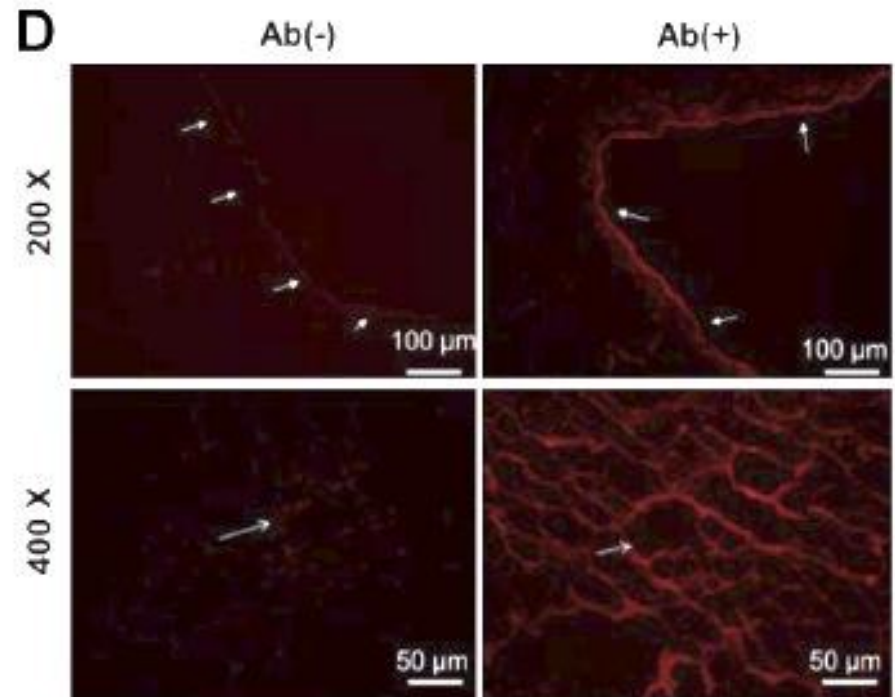
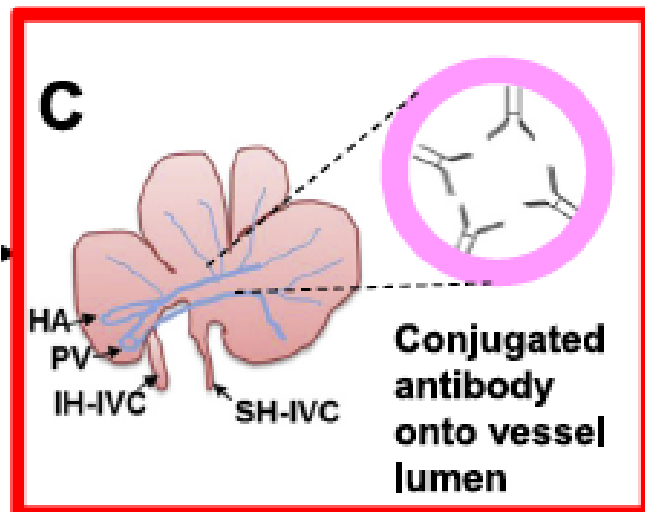
Heparine negatively charged

Thromboresistant after 3h of blood perfusion

After 72h, hepatocytes maintained normal morphology

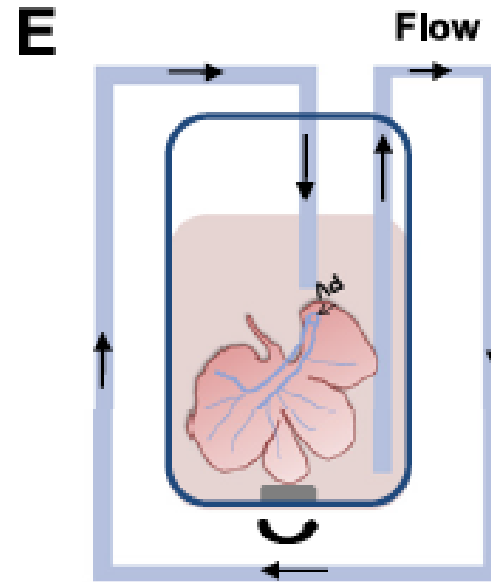
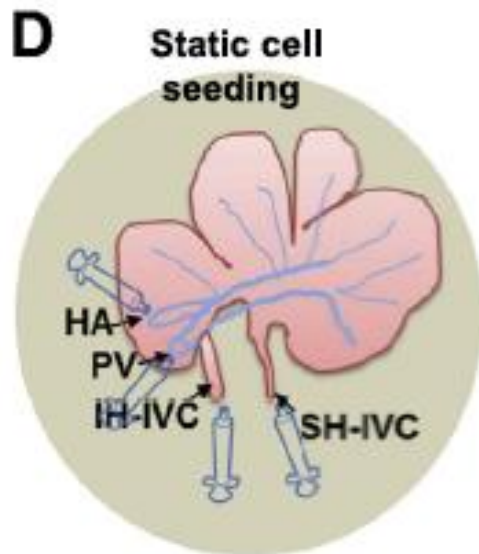
Antibody conjugation method

1. Anti endothelial cell antibodies to stabilize seeded cells on the vessel walls.
Rat anti-mouse CD31 antibody was conjugated to the acellular liver scaffold

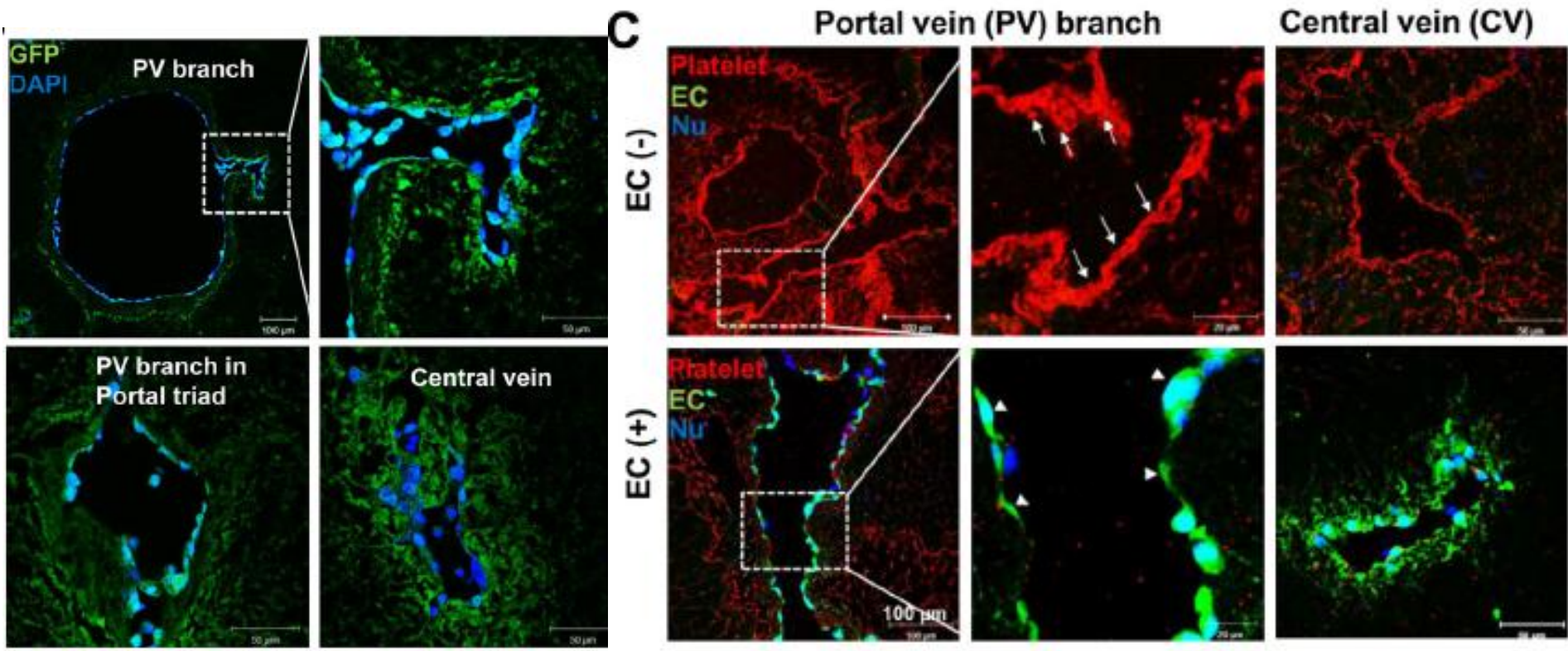


Antibody conjugation method

1. Anti endothelial cell antibodies to stabilize seeded cells on the vessel walls: Rat anti-mouse CD31 antibody was conjugated to the acellular liver scaffold
2. ReEndothelization with endothelial cells (MS1) expressing GFP protein

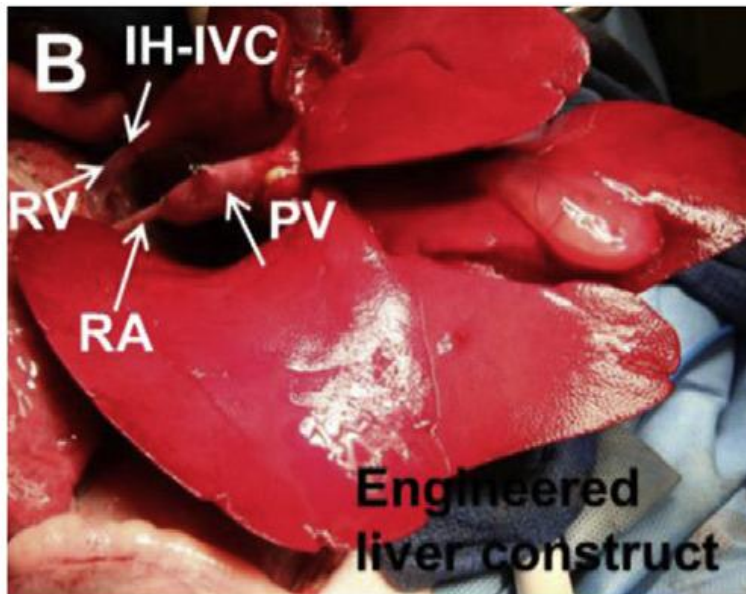


Re-endothelialization characterization



Antibody conjugation method

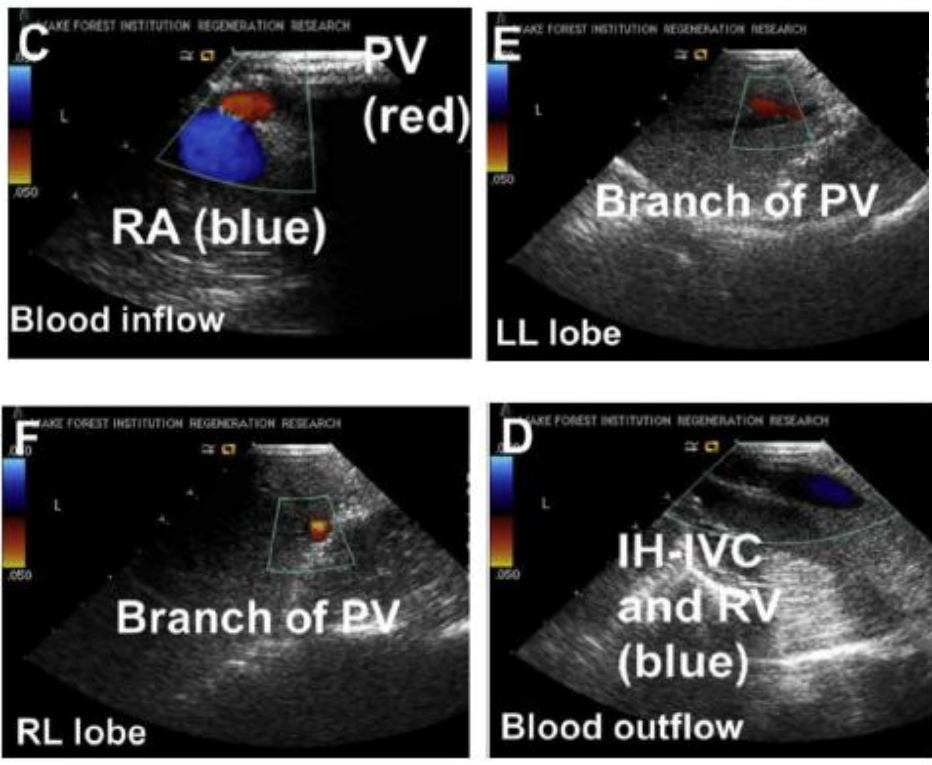
1. Anti endothelial cell antibodies to stabilize seeded cells on the vessel walls: Rat anti-mouse CD31 antibody was conjugated to the acellular liver scaffold
2. ReEndothelization with endothelial cells (MS1) expressing GFP protein
3. Implantation of engineered porcine liver construct



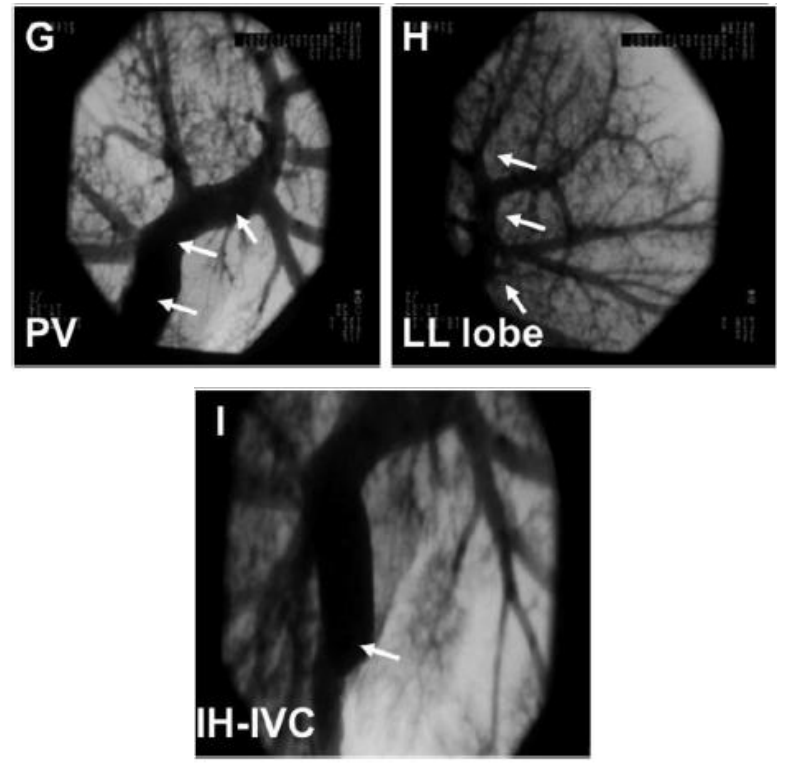
Heterotopically implantation into pig
Left renal artery – Portal vein
Left renal vein - Inferior vena cava

In vivo functional testing

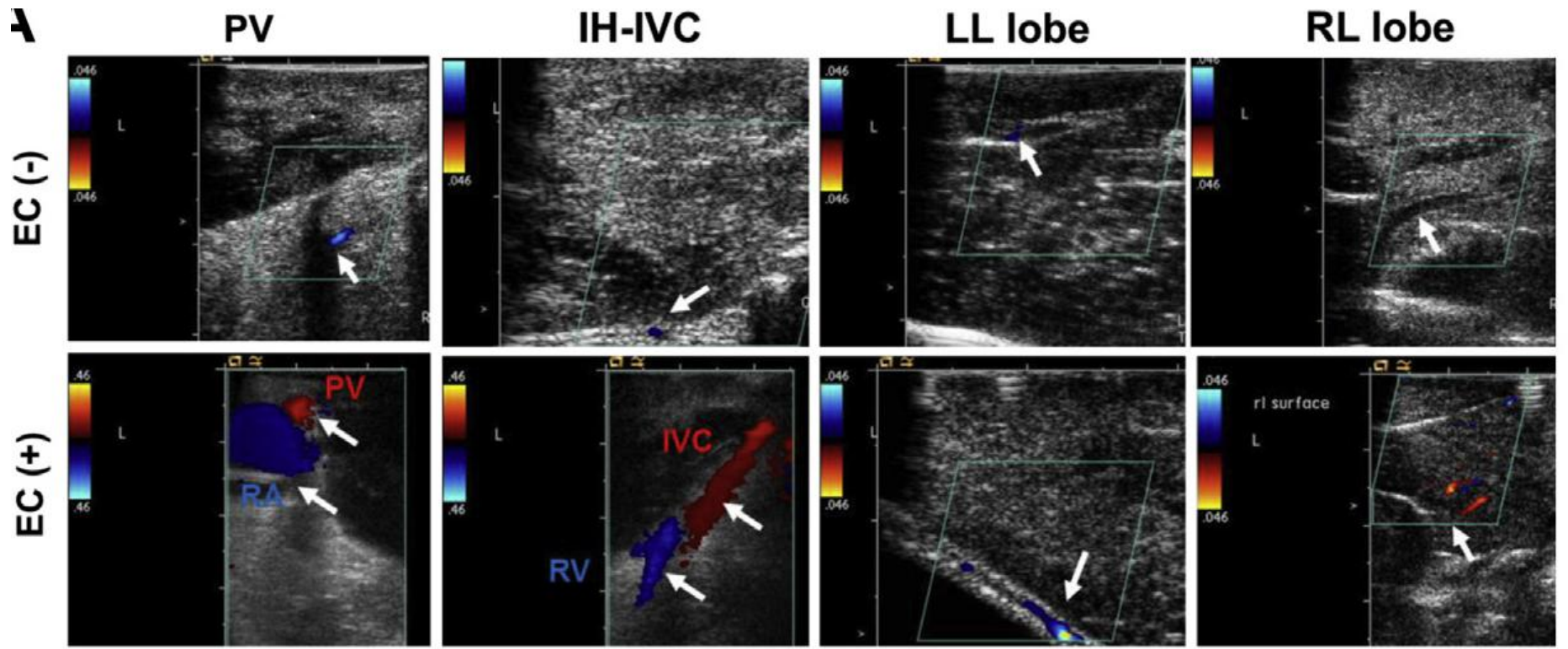
Intraoperative



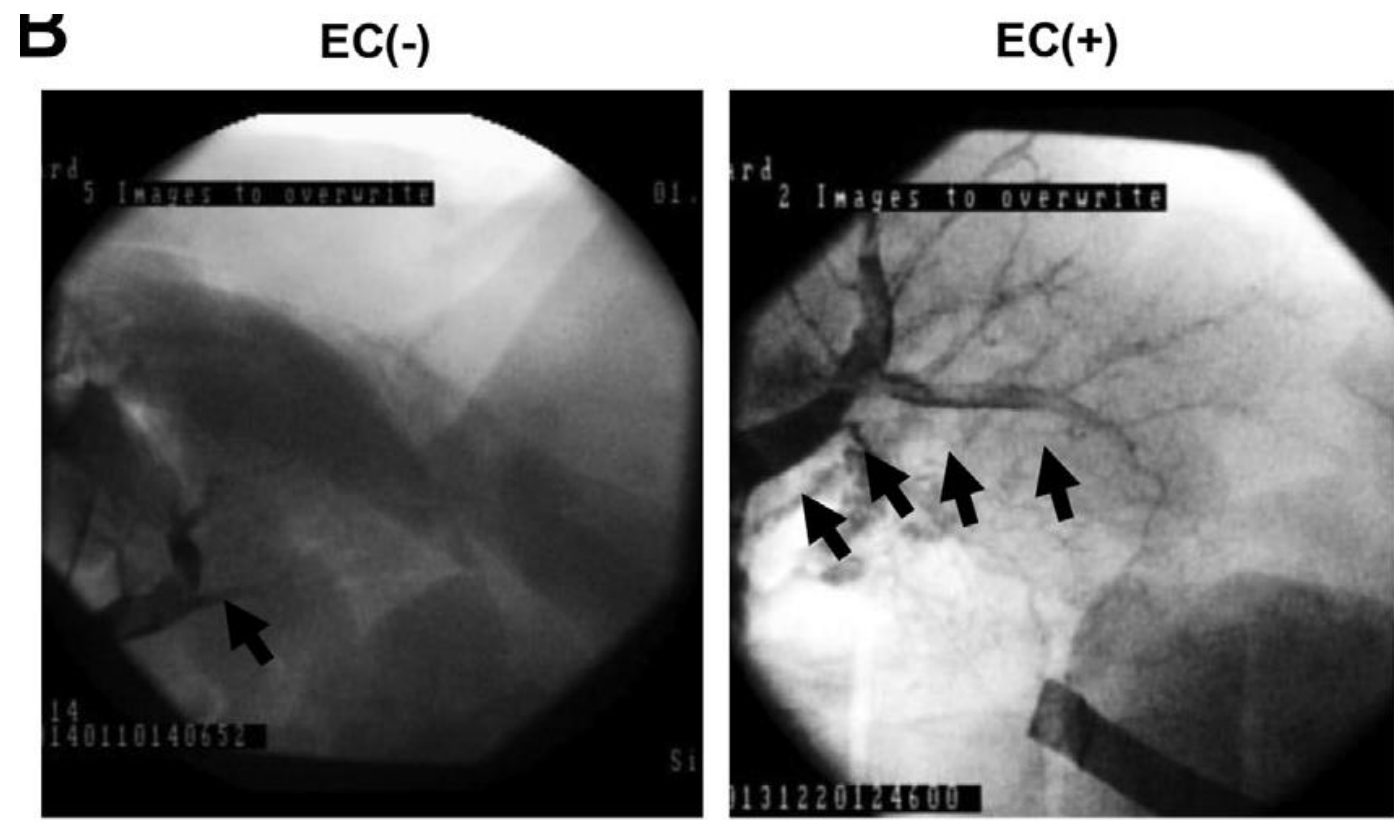
4h after implantation



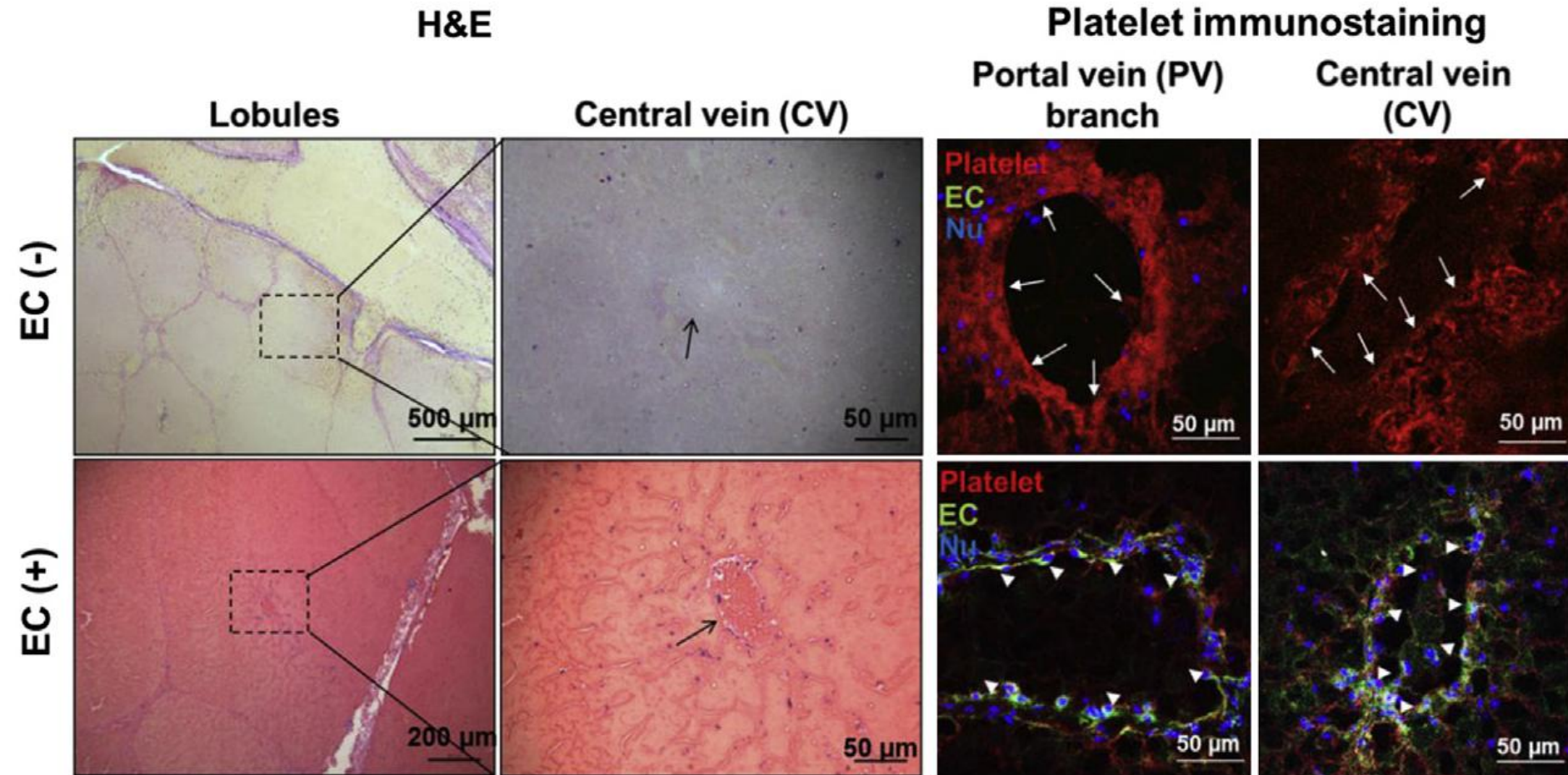
In vivo functional testing: POD 1

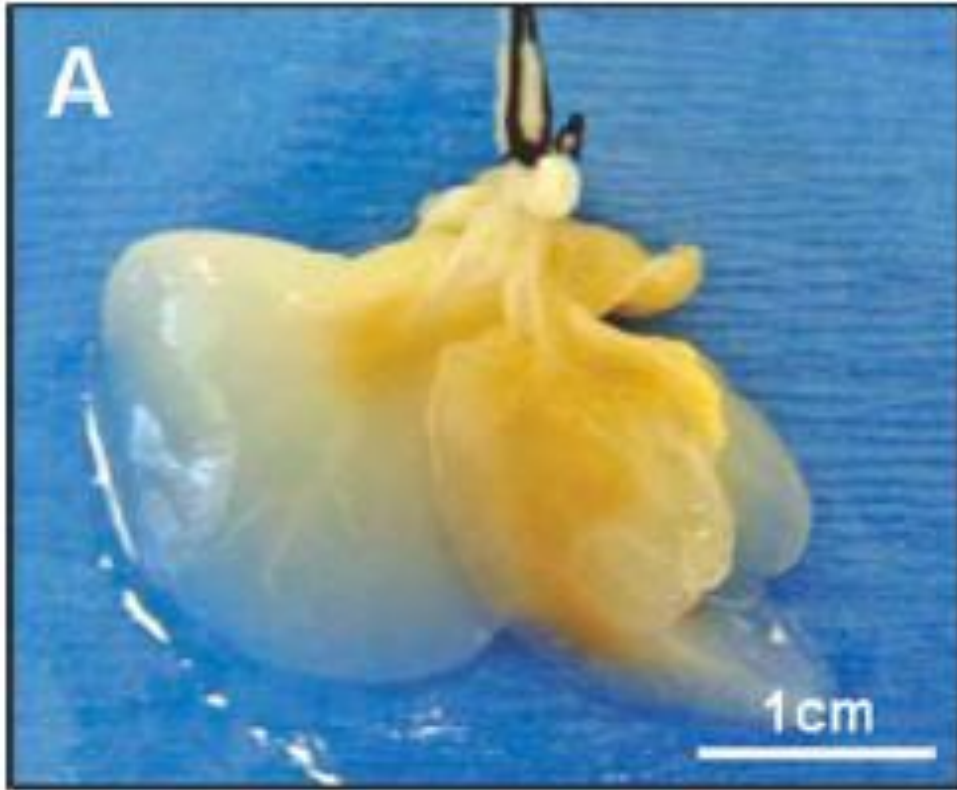


In vivo functional testing: POD 1



In vitro functional testing: POD 1





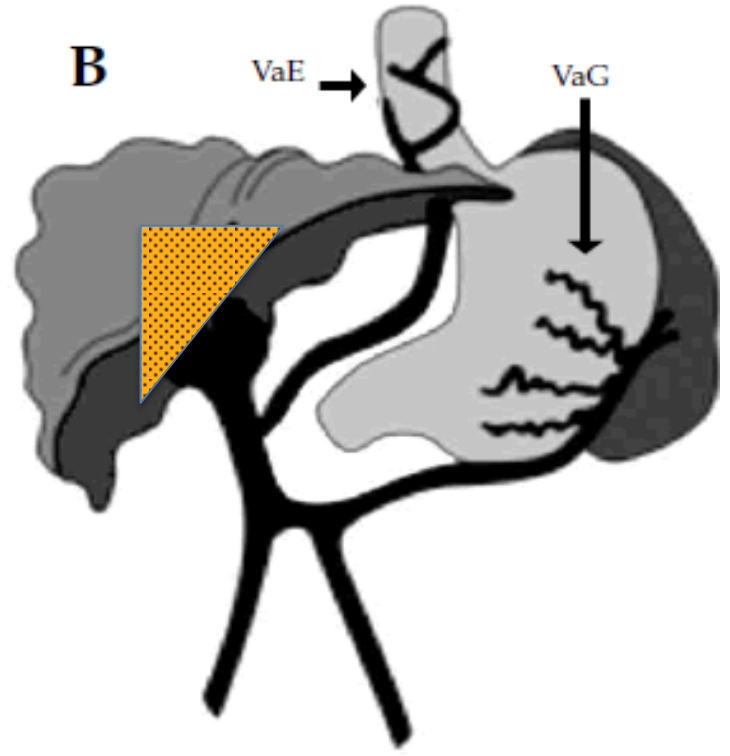
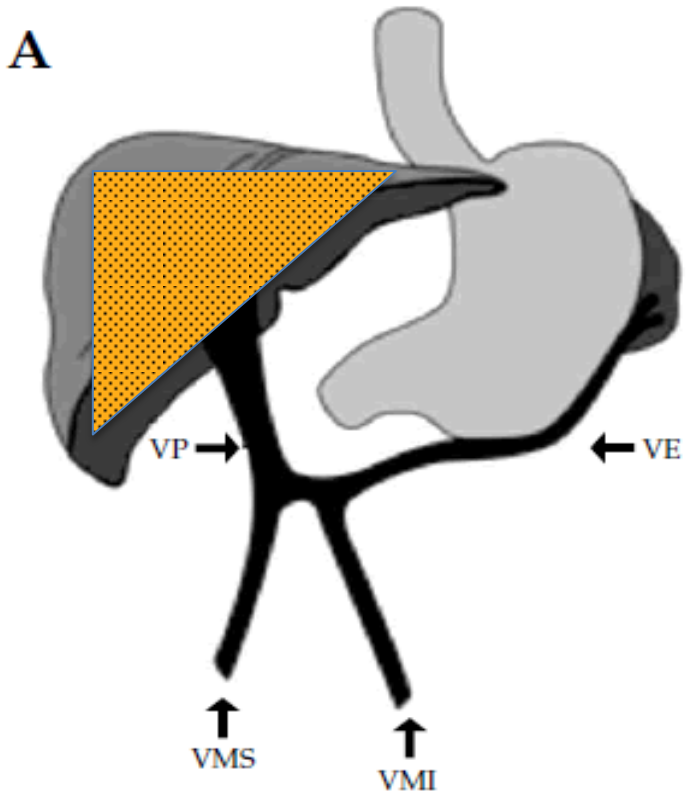
Baptista et al. Hepatology 2010 Nov;12:604-617

70M human fetal hepatocytes

||

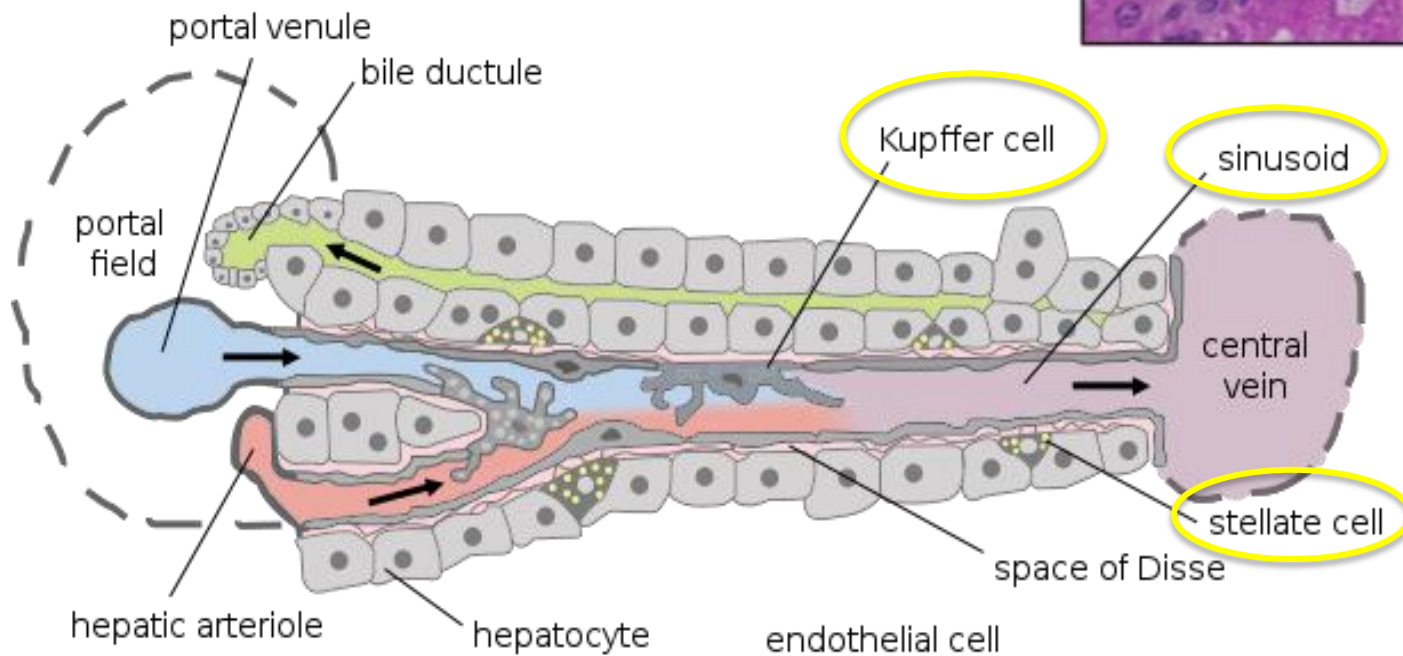
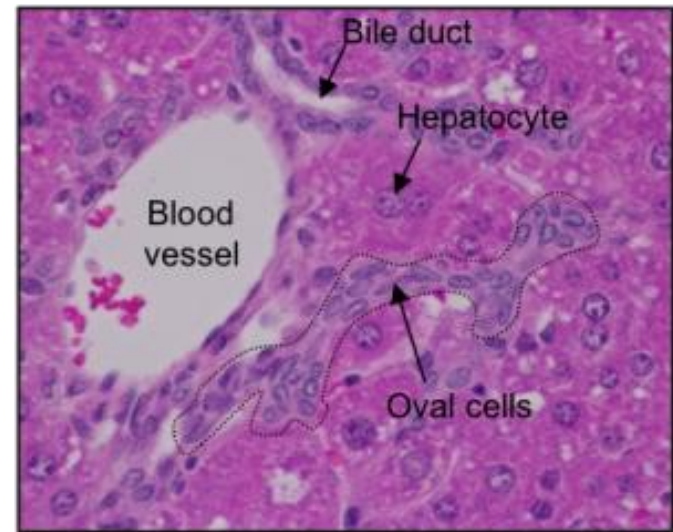
4 livers
(17-21 weeks gestation)

Number is important...

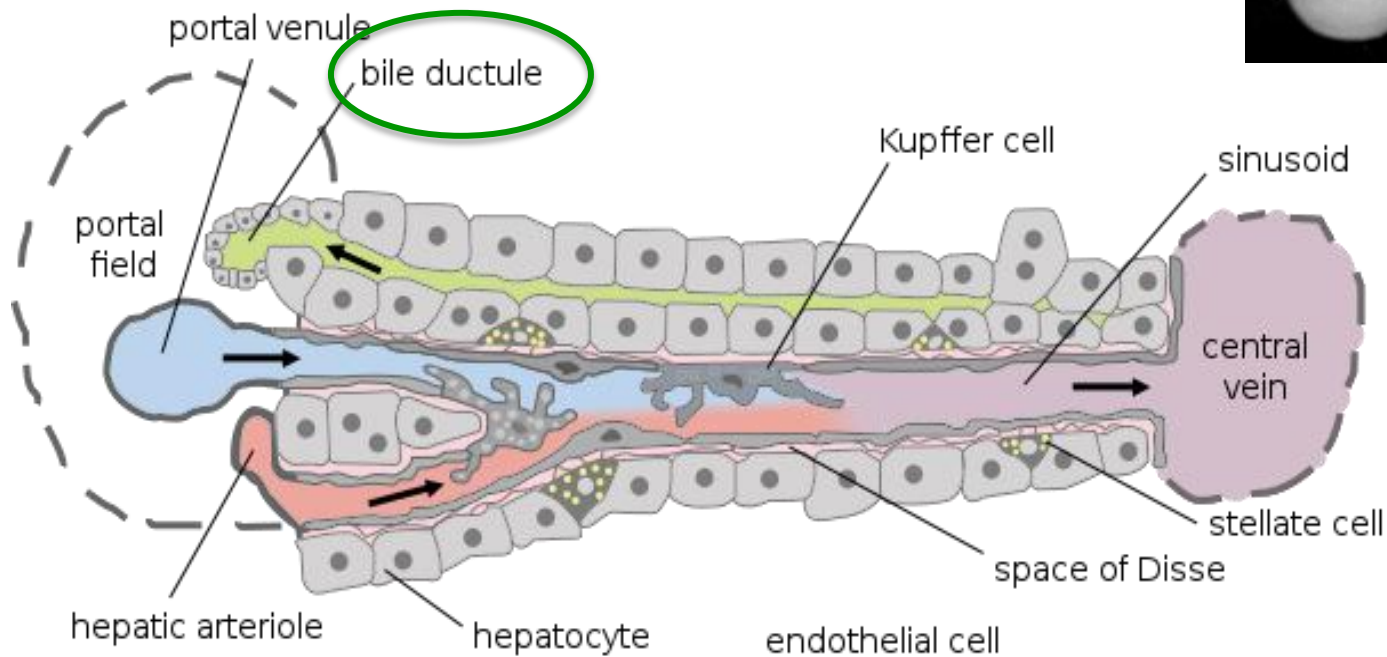


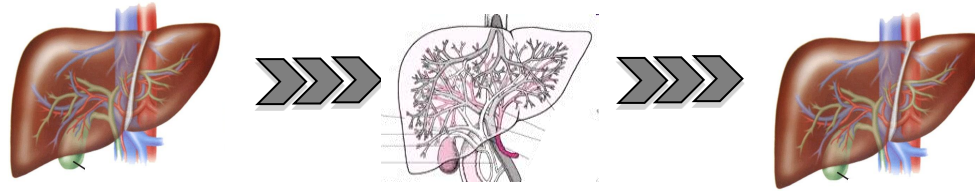
... size is important too

- Co-Culture with other non-parenchymal cells



- Co-Culture with other non-parenchymal cells
- Cholangiocytes - Biliary tree



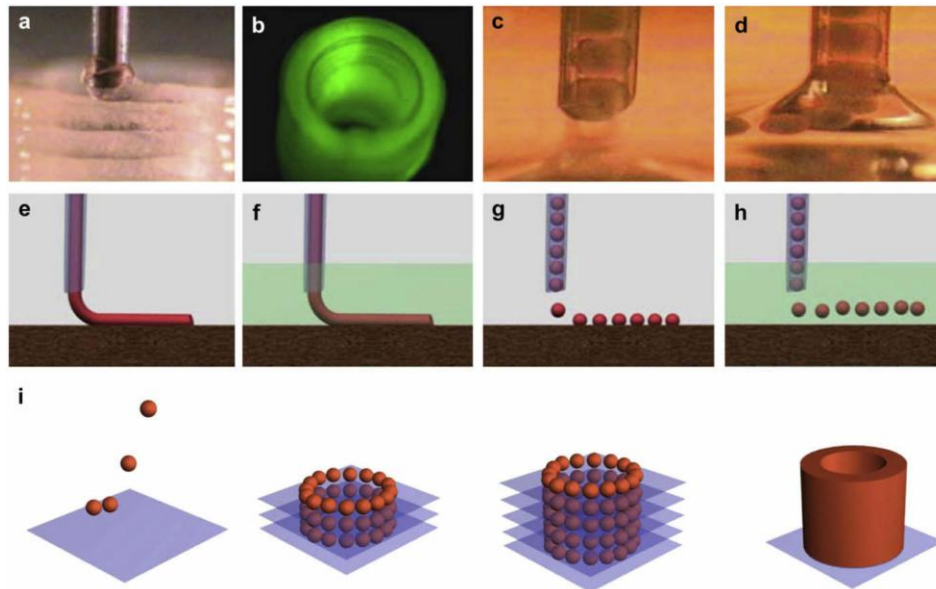


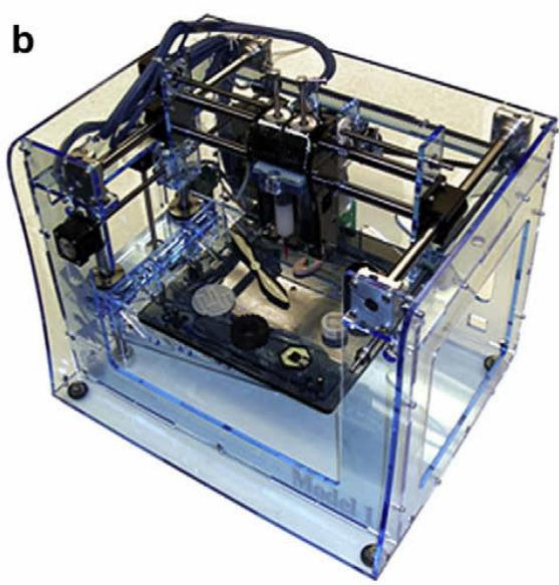
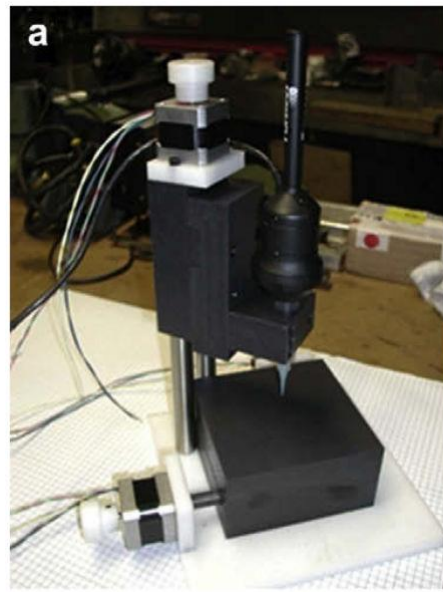
- Decellularized livers are a good option to obtain scaffolds because architecture and vasculature are well preserved
- Cells are “happy” in the scaffolds
 - mature hepatocytes: viable and functional
 - immature cells: differentiate into cells present in the liver
- Multistep recellularization
- Endothelization needed for transplantation
- Main concerns: number of cells and size of organoid
- Future directions:
 - Coculture with other non-parenchymal cells
 - Cholangiocytes and Bile Duct

Organ Bioprinting

Organ Bioprinting: technology to fabricate scaffolds

- Based on the Additive Manufacturing Technology
Technique that produces complex 3D structures being able to control the size, shape, distribution and interconnectivity of pores of the scaffold
- Allow direct cell deposition in organotypic architecture





Mironov. Biomaterials 2009;30(12):2164-2174

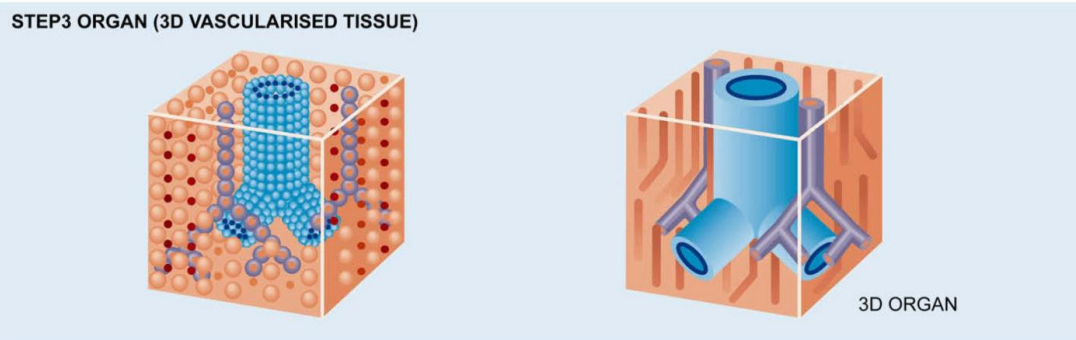
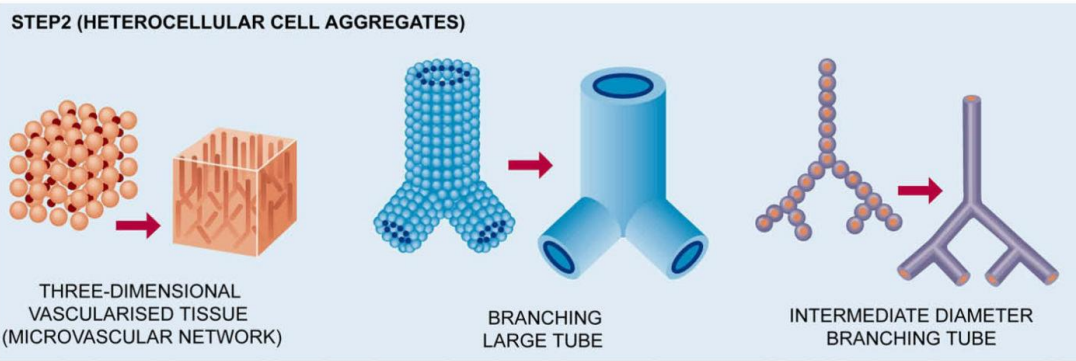
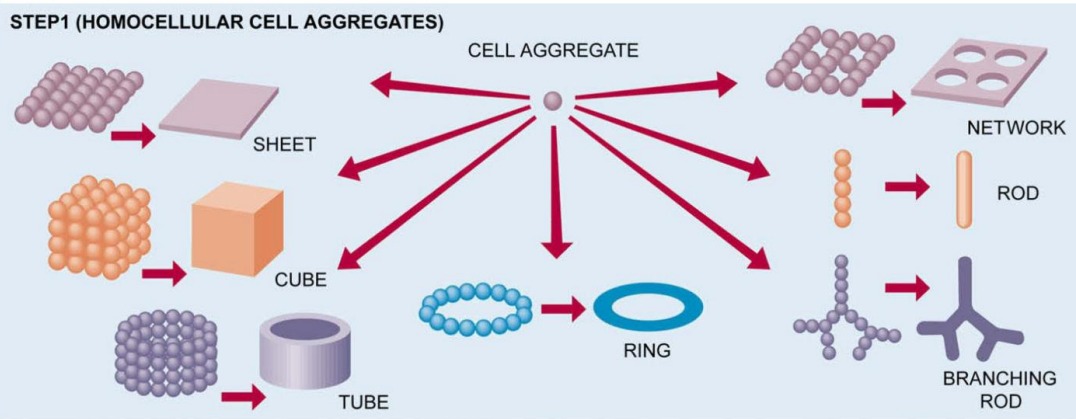


Table 1: Tissue engineering applications using bioprinting technology

Tissue	Techniques	Cell types	Growth factors	Materials
Heart valve	Extrusion-based bioprinting	Aortic valve interstitial cell Aortic root sinus smooth muscle cell	-	Hyaluronic acid Gelatin Alginate
Myocardial tissue Blood vessel	Extrusion-based bioprinting	Cardiomyocyte progenitor cell	-	Alginate
	Jetting-based bioprinting	Endothelial cell Smooth muscle cell Mesenchymal stem cell	-	Fibrin
Musculo-skeletal tissue	Extrusion-based bioprinting	Endothelial cell Cardiac cell Smooth muscle cell Fibroblast	-	Collagen Agarose Alginate
	Jetting-based bioprinting	Muscle-derived stem cells Myoblast Mesenchymal fibroblast	BMP-2 FGF-2	Fibrin
	Extrusion-based bioprinting	Bone marrow stromal cell Endothelial progenitor cell Endogeneous stem cell	TGF- β	Agarose Alginate Hydroxyapatite Polycaprolactone
	Jetting-based bioprinting	Embryonic motoneuron cell Hippocampal cell Cortical cell Neuronal precursor cell Neural stem cells	CNTF VEGF	Soy agar Collagen Fibrin
Nerve	Extrusion-based bioprinting	Bone marrow stem cell Schwann cells	-	Agarose
	Jetting-based bioprinting	Dermal fibroblast Epidermal keratinocyte	-	Collagen

